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E. S. D.

Ref.: Expediente No. 08.116.818
Solicitud de Patente a nombre de
CODMAN & SHURTLEFF, INC.

Yo, JIMENA ESCOBAR URIBE, identificada como aparece al pie de mi firma, domiciliada en la Carrera 11 No. 86-53, piso 6, obrando como apoderada de la sociedad **CODMAN & SHURTLEFF, INC.**, domiciliada en Raynham, Massachussets, Estados Unidos de América, solicitante de la patente de la referencia, atentamente me permito presentar copia certificada de la solicitud de Patente número 11/931.127 presentada en Estados Unidos de América el día 31 de octubre de 2007, con la debida traducción de lo pertinente.

Señor Superintendente,


JIMENA ESCOBAR URIBE
C.C. 39.779.452 de Usaquén
T.P. 68.228
Cod. 5376
/srr

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Número de Solicitud: 11/931,127

Fecha de Presentación: Octubre 31, 2007

El código del país y el número de su solicitud de prioridad para ser usado en presentación en el extranjero bajo la Convención de París, es US11/931,127

Por la autoridad del
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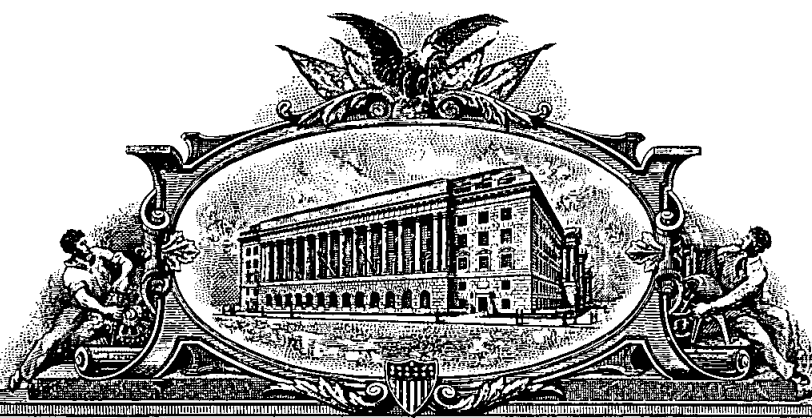
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APPLICATION NUMBER: *11/931,127*

FILING DATE: *October 31, 2007*

THE COUNTRY CODE AND NUMBER OF YOUR PRIORITY APPLICATION, TO BE USED FOR FILING ABROAD UNDER THE PARIS CONVENTION, IS *US11/931,127*

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Certifying Officer

Electronic Acknowledgement Receipt

EFS ID:	2403210
Application Number:	11931127
International Application Number:	
Confirmation Number:	1792
Title of Invention:	Wireless Flow Sensor
First Named Inventor/Applicant Name:	Salim Kassem
Customer Number:	21125
Filer:	Joshua Trevor Matt
Filer Authorized By:	
Attorney Docket Number:	22719-91 (COD5161USNP)
Receipt Date:	31-OCT-2007
Filing Date:	
Time Stamp:	14:47:26
Application Type:	Utility under 35 USC 111(a)

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Document Number	Document Description	File Name	File Size(Bytes) /Message Digest	Multi Part /.zip	Pages (if appl.)
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1	Application Data Sheet	ADS_fill.pdf	1010159	no	4
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Warnings:					
Information:					
2		Application_22719_91.pdf	207148	yes	21
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	Multipart Description/PDF files in .zip description				
	Document Description		Start	End	
	Specification		1	17	
	Claims		18	20	
	Abstract		21	21	
Warnings:					
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3	Drawings-only black and white line drawings	Drawings_22719_91.pdf	366481	no	12
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Warnings:					
Information:					
4	Fee Worksheet (PTO-06)	fee-info.pdf	8451	no	2
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If a timely submission to enter the national stage of an international application is compliant with the conditions of 35 U.S.C. 371 and other applicable requirements a Form PCT/DO/EO/903 indicating acceptance of the application as a national stage submission under 35 U.S.C. 371 will be issued in addition to the Filing Receipt, in due course.

New International Application Filed with the USPTO as a Receiving Office

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Application Data Sheet 37 CFR 1.76		Attorney Docket Number	22719-91 (COD5161USNP)
		Application Number	
Title of Invention	Wireless Flow Sensor		
The application data sheet is part of the provisional or nonprovisional application for which it is being submitted. The following form contains the bibliographic data arranged in a format specified by the United States Patent and Trademark Office as outlined in 37 CFR 1.76. This document may be completed electronically and submitted to the Office in electronic format using the Electronic Filing System (EFS) or the document may be printed and included in a paper filed application.			

Secrecy Order 37 CFR 5.2

☐	Portions or all of the application associated with this Application Data Sheet may fall under a Secrecy Order pursuant to 37 CFR 5.2 (Paper filers only. Applications that fall under Secrecy Order may not be filed electronically.)
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Applicant Information:

Applicant 1					Remove				
Applicant Authority		☒ Inventor		☐ Legal Representative under 35 U.S.C. 117		☐ Party of Interest under 35 U.S.C. 118			
Prefix	Given Name	Middle Name		Family Name		Suffix			
	Salim			Kassem					
Residence Information (Select One)							☒ US Residency	☐ Non US Residency	☐ Active US Military Service
City	North Attleboro		State/Province	MA	Country of Residence	US			
Citizenship under 37 CFR 1.41(b) i			CO						
Mailing Address of Applicant:									
Address 1		1 Stonefield Court							
Address 2									
City	North Attleboro			State/Province		MA			
Postal Code		02760		Country	US				
All Inventors Must Be Listed - Additional Inventor Information blocks may be generated within this form by selecting the Add button.									
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Correspondence Information:

Enter either Customer Number or complete the Correspondence Information section below. For further information see 37 CFR 1.33(a).				
☒ An Address is being provided for the correspondence information of this application.				
Customer Number	21125			
Email Address	jmatt@nutter.com		Add Email	Remove Email

Application Information:

Title of the Invention	Wireless Flow Sensor		
Attorney Docket Number	22719-91 (COD5161USNP)	Small Entity Status Claimed ☐	
Application Type	Nonprovisional		
Subject Matter	Utility		
Suggested Class (if any)		Sub Class (if any)	
Suggested Technology Center (if any)			
Total Number of Drawing Sheets (if any)	12	Suggested Figure for Publication (if any)	

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Application Data Sheet 37 CFR 1.76		Attorney Docket Number	22719-91 (COD5161USNP)
		Application Number	
Title of Invention	Wireless Flow Sensor		

Publication Information:

☐	Request Early Publication (Fee required at time of Request 37 CFR 1.219)
☐	Request Not to Publish. I hereby request that the attached application not be published under 35 U.S.C. 122(b) and certify that the invention disclosed in the attached application has not and will not be the subject of an application filed in another country, or under a multilateral international agreement, that requires publication at eighteen months after filing.

Representative Information:

Representative information should be provided for all practitioners having a power of attorney in the application. Providing this information in the Application Data Sheet does not constitute a power of attorney in the application (see 37 CFR 1.32). Enter either Customer Number or complete the Representative Name section below. If both sections are completed the Customer Number will be used for the Representative Information during processing.

Please Select One:	☒ Customer Number	☐ US Patent Practitioner	☐ Limited Recognition (37 CFR 11.9)
Customer Number	21125		

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Prior Application Status		Remove	
Application Number	Continuity Type	Prior Application Number	Filing Date (YYYY-MM-DD)
Additional Domestic Benefit/National Stage Data may be generated within this form by selecting the Add button.			Add

Foreign Priority Information:

This section allows for the applicant to claim benefit of foreign priority and to identify any prior foreign application for which priority is not claimed. Providing this information in the application data sheet constitutes the claim for priority as required by 35 U.S.C. 119(b) and 37 CFR 1.55(a).

		Remove	
Application Number	Country	Parent Filing Date (YYYY-MM-DD)	Priority Claimed
			☒ Yes ☐ No
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Assignee 1	Remove
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Application Data Sheet 37 CFR 1.76		Attorney Docket Number		22719-91 (COD5161USNP)	
		Application Number			
Title of Invention		Wireless Flow Sensor			
If the Assignee is an Organization check here. ☒					
Organization Name		Codman Shurleff, Inc.			
Mailing Address Information:					
Address 1		325 Paramount Drive			
Address 2					
City		Raynham	State/Province		MA
Country	US	Postal Code		02767	
Phone Number		Fax Number			
Email Address					
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Signature:

A signature of the applicant or representative is required in accordance with 37 CFR 1.33 and 10.18. Please see 37 CFR 1.4(d) for the form of the signature.					
Signature		/Joshua T. Matt/		Date (YYYY-MM-DD)	2007-10-31
First Name	Joshua	Last Name	Matt	Registration Number	55435

This collection of information is required by 37 CFR 1.76. The information is required to obtain or retain a benefit by the public which is to file (and by the USPTO to process) an application. Confidentiality is governed by 35 U.S.C. 122 and 37 CFR 1.14. This collection is estimated to take 23 minutes to complete, including gathering, preparing, and submitting the completed application data sheet form to the USPTO. Time will vary depending upon the individual case. Any comments on the amount of time you require to complete this form and/or suggestions for reducing this burden, should be sent to the Chief Information Officer, U.S. Patent and Trademark Office, U.S. Department of Commerce, P.O. Box 1450, Alexandria, VA 22313-1450. DO NOT SEND FEES OR COMPLETED FORMS TO THIS ADDRESS. **SEND TO: Commissioner for Patents, P.O. Box 1450, Alexandria, VA 22313-1450.**

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WIRELESS FLOW SENSOR

FIELD

[0001] The present application generally relates to devices and methods for non-invasively monitoring and/or measuring the flow of a fluid, and more particularly for monitoring and/or measuring the flow of a fluid in an implantable medical device.

BACKGROUND

[0001] It is often desirable to non-invasively monitor or measure the flow of a fluid, for example in an implanted medical device or in a body, and to be able to communicate or indicate the monitoring or measurement information remotely.

[0002] By way of illustration, treatment of hydrocephalus can involve monitoring the flow rate of cerebrospinal fluid through a hydrocephalus shunt. Hydrocephalus is a neurological condition that is caused by the abnormal accumulation of cerebrospinal fluid (CSF) within the ventricles, or cavities, of the brain. CSF is a clear, colorless fluid that is primarily produced by the choroid plexus and surrounds the brain and spinal cord, aiding in their protection. Hydrocephalus can arise when the normal drainage of CSF in the brain is blocked in some way, which creates an imbalance between the amount of CSF produced by the choroid plexus and the rate at which CSF is absorbed into the bloodstream, thereby increasing pressure on the brain.

[0003] Hydrocephalus is most often treated by surgically implanting a shunt system in a patient. The shunt system diverts the flow of CSF from the ventricle to another area of the body where the CSF can be absorbed as part of the circulatory system. Shunt systems come in a variety of models and typically share similar functional components. These components include a ventricular catheter, which is introduced through a burr hole in the skull and implanted in the patient's ventricle, a drainage catheter that carries the CSF to its ultimate drainage site, and optionally a flow-control mechanism, e.g., shunt valve, that regulates the one-way flow of CSF from the ventricle to the drainage site to maintain normal pressure within the ventricles. It is this flow of CSF which may need to be measured.

[0004] In some cases, measuring the flow of CSF can be accomplished by a flow sensor using temperature differentials between two points, e.g., with a mechanism for heating or cooling the

CSF in a particular section of the catheter. However, it would be advantageous to provide a flow sensor capable of more accurate and/or direct measurements of flow, without the need for heating or cooling equipment, and to provide a straightforward way to retrieve the measurements from the sensor. Such considerations can apply to a wide range of applications involving the measurement of gas and fluid flow, including CSF, within an implanted device or an embedded, encapsulated, or relatively inaccessible space.

[0002] Accordingly, there remains a need for non-invasive monitoring and/or measuring the flow of a fluid, and more particularly for monitoring and/or measuring the flow of a fluid in an implantable medical device.

SUMMARY

[0003] In one embodiment, an exemplary implantable sensor for measuring fluid flow is provided. The implantable sensor can have a sensor housing adapted to receive fluid flow therethrough. In some embodiments, the sensor housing can have a domed portion defining a reservoir therein, and the implantable sensor can measure the flow rate of fluid through the reservoir. A radio frequency tag can be located within the sensor housing. The radio frequency tag can be adapted to interact with a wireless signal and to produce a response to the wireless signal. The implantable sensor can also include a masking element that is disposed in the sensor housing. The masking element and the radio frequency tag can be configured to move relative to one another, for example the masking element moving, the radio frequency tag moving, or both, to alter the response of the radio frequency tag and thereby indicate a rate of fluid flowing through the sensor housing. The masking element, for example, can include a conductive member that alters the response of the radio frequency tag by covering at least a portion of it. The response of the radio frequency tag can have at least one characteristic, such as a resonant frequency, harmonic spectra, decay characteristic, and Q factor, that corresponds to the flow rate. In some embodiments, the implantable sensor can also have a valve assembly that is in fluid communication with the sensor housing and that is adapted to control a rate of fluid flowing through the sensor housing.

[0004] A wide array of variations are possible. The radio frequency tag can include a disk having an asymmetrical antenna, and the masking element can be configured to mask at least

part of the antenna. In some embodiments, the radio frequency tag can also include a chip for storing data and an antenna adapted to communicate the stored data to an external reading device.

[0005] Various techniques can be used to associated the radio frequency tag with the flow rate. For example, the masking element can be configured to rotate in response to the flow rate of fluid through the sensor housing. For example, the masking element can include a disk formed at least in part of a conductive material and configured to rotate around an axis thereof. The masking element can be configured to rotate around an axis thereof to mask different parts of the radio frequency tag such that the response of the radio frequency tag to the wireless signal is periodic. The rotation can selectively mask part of the radio frequency tag such that the response of the radio frequency tag to the wireless signal is periodic. The conductive material can be in the form of, for example, a spiral or a plurality of discrete conductive sections. In other embodiments, the masking element can include a disk having a pattern of conductive material formed thereon and a biasing element, such as a spring, calibrated to resist rotation of the disk caused by the flow rate of fluid through the sensor housing. Alternatively, the masking element can have a wedge formed at least in part of a conductive material and the masking element can be configured to translate in relation to the flow rate of fluid through the sensor housing.

[0006] In another embodiment, an implantable sensor is provided which has a sensor housing adapted to receive fluid flow therethrough, and a conductive member disposed within the valve assembly. The conductive member can be configured to selectively cover at least a portion of a radio frequency tag and thereby alter a response thereof to a wireless signal to indicate a rate of fluid flowing through the sensor housing. The response of the radio frequency tag can have at least one measurable characteristic, such as resonant frequency, harmonic spectra, decay characteristic, and Q factor, that can indicate the flow rate. In some embodiments, the frequency tag can be configured to move relative to the conductive member, which can result in the frequency tag being selectively covered. The radio frequency tag can also include a disk having an asymmetrical antenna formed thereon. In other embodiments, the conductive member can be configured to move relative to the radio frequency tag, which can result in the frequency tag being selectively covered. The conductive member can form part of a rotatable disk, for example. In some embodiments, the implantable sensor can include a valve assembly that is in

fluid communication with the sensor housing and that is adapted to control the rate of fluid flowing through the sensor housing.

[0007] In other aspects, an exemplary method for measuring fluid flow is provided and can include positioning a sensor housing between an inlet tube and an outlet tube, the sensor housing having a radio frequency tag disposed therein. The method can further include transmitting a wireless signal to the radio frequency tag from a reading device, and wirelessly receiving a response from the radio frequency tag that indicates a rate of fluid flowing through the sensor housing. In some embodiments, the response can change in relation to the rate of fluid flowing through the sensor housing, and/or it can include a periodic signal. The method can also include analyzing the response to detect any of resonant frequency, harmonic spectra, decay characteristic, and Q factor of an antenna included in the radio frequency tag, and/or receiving a response from the radio frequency tag that communicates data previously stored therein.

[0008] In other embodiments, the method can further include coupling the inlet tube to a catheter within a patient's ventricle, and coupling the outlet tube to a drainage catheter for draining the patient's cerebrospinal fluid. The method can also include coupling the sensor housing to a valve assembly adapted to control a rate of fluid flowing through the sensor housing.

BRIEF DESCRIPTION OF THE DRAWINGS

[0009] Various exemplary embodiments disclosed herein will be more fully understood from the following detailed description taken in conjunction with the accompanying drawings, in which:

[0010] FIG. 1A is a top view of one exemplary implantable valve suitable for use in a hydrocephalus shunt and including a flow sensor.

[0011] FIG. 1B is a schematic view of one exemplary embodiment of an implantable sensor having a housing with a radio frequency tag and a masking element disposed therein for measuring the flow of a fluid therethrough;

[0012] FIG. 2A is a top view of one exemplary embodiment of a radio frequency tag and a masking element for use with the implantable sensor shown in FIG. 1B;

[0013] FIG. 2B is a top view of the radio frequency tag and masking element shown in FIG. 2A following rotation of the masking element;

[0014] FIG. 3 is a schematic view of an exemplary configuration for coupling the flow of a fluid to a radio frequency tag and/or masking element to cause rotation thereof;

[0015] FIG. 4 is a graph illustrating amplitude vs. frequency characteristics of an exemplary response from a radio frequency tag in an implantable sensor;

[0016] FIG. 5 is a top view of another embodiment of a radio frequency tag and a masking element;

[0017] FIG. 6 is a top view of another embodiment of a radio frequency tag and a masking element;

[0018] FIG. 7A is a top view of another embodiment of a radio frequency tag and a masking element;

[0019] FIG. 7B is a top view the radio frequency tag and masking element shown in FIG. 7A following translation of the masking element and/or radio frequency tag;

[0020] FIG. 8 is a schematic view of an exemplary configuration for coupling the flow of a fluid to a radio frequency tag and/or masking element to cause translation thereof;

[0021] FIG. 9A is a schematic diagram of one exemplary model of a circuit having resonance characteristics;

[0022] FIG 9B is a graph of an output voltage signal as a function of frequency for the circuit shown in FIG. 9A;

[0023] FIG 9C is a graph of an output voltage signal as a function of frequency for the circuit shown in FIG. 9A;

[0024] FIG. 10 is a perspective view of an exemplary reading device for reading a flow rate from an implantable sensor; and,

[0025] FIG. 11 illustrates the implantable sensor shown in FIG. 1 implanted in a body and being read by the reading device shown in FIG. 10.

DETAILED DESCRIPTION

[0026] Certain exemplary embodiments will now be described to provide an overall understanding of the principles of the structure, function, manufacture, and use of the devices and methods disclosed herein. One or more examples of these embodiments are illustrated in the accompanying drawings. Those skilled in the art will understand that the devices and methods specifically described herein and illustrated in the accompanying drawings are non-limiting exemplary embodiments and that the scope is defined solely by the claims. The features illustrated or described in connection with one exemplary embodiment may be combined with the features of other embodiments. Such modifications and variations are intended to be included within the scope of the present application.

[0027] The present application generally provides methods and devices for non-invasively measuring or quantifying the flow of a fluid through a device and for indicating that information to another device, e.g., telemetrically. The methods and devices are particularly useful in the context of implantable devices, such as hydrocephalus shunts and associated valves. While the description herein sometimes refers to hydrocephalus shunts, one skilled in the art will understand that the devices and methods described herein can be used in a wide variety of methods and devices in which it is desirable to measure fluid flow.

[0028] FIG. 1A illustrates one exemplary embodiment of an implantable sensor in the context of an implantable valve for a hydrocephalus shunt. As shown, the implantable valve 101 can include a housing 102 with proximal and distal ends 104a, 104b for receiving fluid flow (such as CSF) therethrough between an inlet port 106 and an outlet port 110. The housing 102 can have virtually any configuration, shape, and size. In many embodiments, the size and shape of the housing 102 can be adapted for implantation in a body, e.g., subcutaneous implantation. In the embodiment shown in FIG. 1A, the housing 102 has a substantially linear configuration with a reservoir 108 having a larger area than the ports 106, 110 which can be advantageous for checking the shunt's patency, tapping the CSF, or to administer therapy. The reservoir 108 can also house a flow sensor, as will be described in more detail below, and can also house a

pressure sensor for measuring the pressure of fluid in the reservoir. For example, suitable pressure sensors are described in co-pending, commonly assigned U.S. Patent Application No. 10/907,665, entitled "Pressure Sensing Valve" by Mauge et al., filed April 11, 2005 (now published as U.S. Publication No. 2006-0211946 A1), filed herewith, and in U.S. Patent No. 5,321,989, U.S. Patent No. 5,431,057, and EP Patent No. 1 312 302, the teachings of all of which are hereby incorporated by reference in their entireties. The implantable valve 101 can also include a valve assembly 112 for controlling the flow of fluid through the valve 101 according to remotely or telemetrically selectable settings. A coating can be disposed over the valve 101. Further information on implantable valves can be obtained from U.S. Publication No. 2006-0211946 A1, referenced above.

[0029] FIG. 1B schematically illustrates one exemplary embodiment of an implantable sensor in the housing 102. Fluid (e.g., CSF) can flow as indicated by directional arrows through the housing 102 from an inlet (fluid entry) port 106 at the proximal end 104a, through a reservoir 108, and out an outlet (fluid exit) port 110 at the distal end 104b. The reservoir 108 is not necessary (for example, the housing can be in the form of a catheter or tube), but can be advantageous for accommodating other components of the sensor or device therein. The sensor 100 can also have a radio frequency (RF) tag 114 disposed in the reservoir 108, a masking element 115 associated with the RF tag 114 (for clarity, the RF tag 114 and the masking element 115 are represented together in FIG. 1B, although they need not be one component, or be similarly sized and oriented). Moreover, while the RF tag and masking element are shown disposed within the reservoir 108, they can be positioned at any location within a fluid system as long as they can be used to indicate a flow rate of fluid in the system. As will be described in more detail below, the RF tag 114 and the masking element 115 can be configured to move relative to one another in response to and/or in relation to the rate of flow of fluid through the housing, and to indicate the rate of fluid flow to an external reading device. In some embodiments, the RF tag 114 can further store data, such as identification information (for example, for the sensor and/or for the patient) and flow rate history, which can be communicated to the external reading device. While not shown, the housing 102 can also contain a valve assembly for controlling the flow of fluid from the inlet port 106 to the outlet port 110, the sensor 100 measuring the controlled flow of fluid therethrough. The proximal and distal ends 104a, 104b of the sensor 100 can each be open and adapted to couple to another medical device, such as a catheter.

[0030] The masking element can have a wide variety of configurations and it can be adapted to interact with the RF tag in a variety of ways. FIG. 2A shows one exemplary embodiment of a masking element 115 associated with an RF tag 114 in which the masking element 115 is in the form of a disk with a conductive portion 202 and a non-conductive (or differently conductive) portion 208. The conductive portion 202 can be a material, such as silver, gold, copper, aluminum, or others known in the art, etc., deposited on the disk. The conductive portion 202 can also be attached or coupled to the disk, or it can be a non-circular portion that fits together with a non-conductive portion 208 to form the complete disk, and so on. The conductive portion 202 can have a variety of shapes, but as shown it is in the shape of a spiral. Alternatively, the conductive portion can be in the shape of a strip of varying width, can have one or more discrete portions of varying size (e.g., a plurality of discrete rectangular shapes), and can have virtually any size and shape that is rotationally asymmetric. As shown in FIG. 2A, the RF tag 114 can be disposed behind the masking element, and particularly behind the spiral portion formed of conductive material 202. (In other embodiments, the RF tag can be disposed behind or in front of the masking element.) In use, the flow of a fluid through a housing 102, such as is shown in FIG. 1, can cause rotation of the masking element 115 about the central axis 206, while the RF tag 114 can remain fixed (for example, fixed relative to the housing shown in FIGS. 1A-1B). FIG. 2B illustrates one possible result of such relative movement. As shown in FIG. 2B, following rotation of the masking element 115, a narrow portion of the conductive material 202 covers the RF tag 114. Accordingly, the response of the RF tag 114 to an external signal (e.g., from a reading device emitting a signal at one or more radio frequencies) in FIG. 2A can differ from that of FIG. 2B and can indicate such relative position and/or movement. For example, in some embodiments, a characteristic of the response of the RF tag 114, such as resonance frequency, harmonic spectra, decay characteristics, or Q factor, can change depending on the relative position or motion of the masking element 115 and the RF tag 114, to indicate the flow rate of fluid within the sensor housing.

[0031] In some embodiments, the masking element 115 can rotate around its central axis 206 at a speed relative to the RF tag 114 to indicate a fluid flow rate. For example, as shown in FIG. 3, an element 300 can be coupled to fluid flowing in direction 302 in a housing 102 via surface features 304 formed on the element 300, causing the element 300 to rotate as shown by arrow 306. The element 300 can be a masking element 115 itself or alternatively it can be coupled to

the masking element 115, for example, via a shaft, gears, and so on. The resulting relative motion of the masking element 115 and the RF tag 114 can be manifested as a periodic radio frequency signal, such as is shown in FIG. 4. The period of the signal (for example, the periodicity of the $f_{\max}$ peaks in FIG. 4, or other metric) can be correlated to the flow rate of the fluid.

[0032] It should be understood that in some embodiments the nature of the rotation of the masking element 115 relative to the RF tag 114 can vary and can be used to sense or measure other characteristics. In some embodiments, in response to a pressure from flowing fluid the masking element 115 can rotate to a position relative to the RF tag 114 and stop. For example, as shown in FIG. 3, a spring 308 can be disposed on the rotational axis of element 300 to resist the rotation thereof, and the spring 308 can be calibrated such that a given force or pressure causes a known degree of rotation, or rotational deflection, in the element 300. The resulting relative position of the masking element 115 and the RF tag can indicate the pressure via the response of the RF tag to a radio frequency signal, as described above.

[0033] The masking element 115 and the RF tag 114 shown in FIG. 1B can have a wide variety of other configurations. For example, FIG. 5 shows an exemplary masking element 500 in the form of a disk which includes a conductive portion 504 disposed within a disk of non-conductive, or differently conductive, material 508. As shown, the conductive portion 504 is in the form of a circle sized to cover the RF tag 502 completely, although in other embodiments, the conductive portion can be adapted to cover the RF tag 502 partially. The masking element 500 can be coupled to flowing fluid so as to rotate around a central axis 506 in relation to the rate of flow, as previously described. Rotation of the masking element 500 can result in a periodic sudden change or discontinuity in the RF tag's response and thereby indicate the flow rate.

[0034] In another embodiment, shown in FIG. 6, a masking element 600 can be in the form of a rectangle, square, or virtually any other shape, and it can be associated with an RF tag 602 having an asymmetric shape. For example, the RF tag 602 can be in the form of a disk with a rotationally asymmetric antenna pattern formed thereon. The pattern can include, for example, antenna lines with varying width, spacing, orientation, and so on. The masking element 600 can be fixed within the housing, and the disk forming the RF tag 602 can be coupled to flowing fluid,

e.g., in the housing as shown in FIG. 1B, so as to rotate around axis 604 in relation to the flow rate, as previously described. Such rotation can cause a change or variations in the response of the RF tag 602 as the conductive masking element 600 covers different portions of the asymmetric antenna of the RF tag 602. As previously mentioned, the response can have characteristics, such as resonance frequency, harmonic spectra, decay characteristics, and/or Q factor, which can change as a result of such rotation and which can be detected in the response of the RF tag 602 to a radio frequency signal emitted by a reading device. In an alternative embodiment, the RF tag 602 can be fixed within the housing and the masking element 600 can be adapted to rotate around an axis or otherwise move relative to the RF tag 602.

[0035] In yet another embodiment, the masking element can be configured to translate relative to the RF tag. For example, FIG. 7A shows a masking element 700 formed of a conductive material in the shape of a wedge and associated with an RF tag 702. As the masking element 700 translates relative to the RF tag 702, it covers a different portion of the RF tag 702 (for example as shown in FIG. 7B), resulting a measurable difference in the RF tag's response, as previously described. The masking element 700 can be coupled to the flow of fluid through the sensor housing in a variety of configurations. For example, the configuration described above in connection with FIG. 3 can be adapted such that rotation of the element 300 causes translation of the masking element 700, for example via a rack and pinion gearing.

[0036] Alternatively, as shown in FIG. 8, a sliding element 800 can be disposed in a housing 102. The sliding element 800 can be configured to receive a force of fluid flowing in direction 802 against a proximal end 804 thereof or against elements 806, and to translate in response thereto. A spring 808 or other biasing element can be configured to provide a force against a distal end 810 of the sliding element 800 that resists the force presented on the sliding element 800 by flowing fluid, and the spring 804 can be calibrated such that the deflection of the sliding element 800 corresponds to a force or pressure from the fluid flow. The sliding element 800 can be coupled to a masking element, such as masking element 700, to effect translational movement thereof.

[0037] As one skilled in the art will appreciate, the masking element and the RF tag can have a wide variety of further configurations, including virtually any configuration in which a masking

element and an RF tag move relative to one another to measure a rate of fluid flow and/or pressure. For example, in some embodiments a variety of masking element shapes can be provided, in some embodiments only one or both of the masking element and the RF tag can be configured to move relative to the other, and so on. In some embodiments, the masking element can physically contact the circuit of the RF tag to thereby change its properties (resistance, capacitance, inductance, etc.) and/or alter connections between conductive elements on the RF tag, for example connecting conductive branches of a circuit, or breaking such connections. In other embodiments, the masking element covers or is disposed in between the reading device and the RF tag. The location of the RF tag and masking element can vary within the housing and are not limited to those shown in the illustrated embodiments. In addition, any mechanism suitable to convert the flow of a fluid to rotational or translational movement can be provided, the foregoing embodiments being by way of example only. Further, many of the embodiments described herein can be adapted to determine or can be correlated to a pressure of fluid in a housing rather than a flow rate.

[0038] Returning to FIGS. 1A-1B, the shape, technical specifications, and size of the RF tag 114 can vary widely. In many embodiments, a relatively small RF tag can be used so as to minimize the footprint of the tag in the device, for example with dimensions in a range of about 5mm to 10mm, but in other embodiments, tags with dimensions of about 3mm to 50 mm can be used and any size is possible.

[0039] It should be understood that in many embodiments, the RF tag 114 can be chipless, and its physical/electromagnetic parameters can be used to determine a flow rate. The RF tag 114 need not have the capability to store data or to communicate according to a protocol, and need not have processing circuitry or digital logic. A chipless RF tag can provide a circuit (for example, having measurable characteristics, such as a tank circuit) and can be powered from the reading device signal. Such an RF tag can be advantageous due to its relatively low power requirements, and need not have the ability to communicate stored data or "identify" itself. However, in other embodiments the RF tag 114 can be chip-based, and can provide data storage for storing additional information related to the application. An example of chip-based tags are the commonly used RF identification tags. Some of these RF identification tags provide minimal information (such as a TRUE or FALSE value), while others can store several bytes of data. A

chip-based RF tag can include processing circuitry, digital logic, a separate antenna, and/or a battery. For example, the RF tag 114 can include a memory for storing data related to the patient and/or sensor. By way of non-limiting example, the RF tag 114 can store sensed pressure data, sensor identification information (e.g., implantation date, sensor type, and sensor identifier code), sensor calibration data, historical data stored from the sensor, tag identification information (e.g., implantation date, tag type, and tag identifier code), and/or patient data (e.g., desired CSF flow rate, previous sensor measurements, and patient medical history). An external reading device, described further below, can read and/or store data in such an RF tag 114.

[0040] The RF tag 114 can have any shape, such as elliptical (including circular) or rectangular (including square), and can have virtually any size. The following table lists, by way of example only, available RF tags suitable for use with the devices and methods described herein. Passive as well as semi-passive and active tags can be used, although semi-passive and active tags sometimes are larger than passive tags because they may have an internal battery, e.g., for power purposes.

Tag Type	Frequency					
	125 KHz	5-7 MHz	13.56MHz	303/433 MHz	860-960 MHz	2.45 GHz
Passive	ISO11784/5, 14223	ISO10536	(ISO15693)	--	ISO18000-6	ISO18000-4
	ISO18000-2	iPico DF/iPX	(ISO15693) MIFARE (ISO14443) Tag-IT (ISO15693) ISO18000-3		Electronic Product Code ("EPC") Class 0 EPC Class 1 EPC GEN II Intellitag tolls (Title 21) rail (Association of American Railroads ("AAR") S918)	Intellitag μ -chip
Semi-Passive	--	--	--	--	rail (AAR S918) Title 21	ISO18000-4 Alien BAP

Active	--	--	--	Savi (American National Standards Institute ("ANSI") 371.2) ISO18000-7 RFCode	--	ISO18000-4 WhereNet (ANSI 371.1)
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Table 1

[0041] By way of further explanation, one exemplary circuit for modeling an RF tag can be generally represented by a resonator circuit 900 as shown in FIG. 9A. The circuit 900 includes a capacitor 902, an inductor 904, and an intrinsic resistance 906. When the RF tag is embedded in a sensor and associated with a masking element, as described above, shifts in the resonant frequency of the circuit 900 can be monitored on a continuous or intermittent basis to measure a rate of fluid flow through the housing. The resonant frequency of the circuit 900 can be detected in a variety of ways, such as by measuring power reflected from the circuit 900 or measuring decaying circulating power of the circuit 900 following a outside signal (e.g., from a reading device). FIG. 9B illustrates an example of a graph showing an output signal of the circuit 900 when introduced to an outside signal. The reflected power of the circuit 900 is at a minimum at the resonant frequency, where ω can be expressed as:

$$\omega = 2\pi f = \frac{1}{\sqrt{LC}}$$

with f representing the resonant frequency, L representing inductance of the inductor 904, and C representing capacitance of the capacitor 902. FIG. 9C illustrates another example of a graph showing an output signal of the circuit 900 when introduced to an outside signal. The reflected power of the circuit 900 in this example is at a maximum at the resonant frequency. Further examples of such RF tags and information on the use of them, including techniques for interrogating them, can be obtained from U.S. Patents No. 6,025,725, and 6,278,379, and U.S. Patent Application Publication No. 2004/0134991, all of which are hereby incorporated by reference in their entireties.

[0042] Referring again to FIGS. 1A-1B, the housing 102 can be formed from a variety of materials. In one exemplary embodiment, however, the housing 102 is formed from a flexible, biocompatible material. Suitable materials include, for example, polymers such as silicones, polyethylene, and polyurethanes, all of which are known in the art. The housing 102 can also optionally be formed from a radio-opaque material. A person skilled in the art will appreciate that the materials are not limited to those listed herein and that a variety of other biocompatible materials having the appropriate physical properties to enable the desired performance characteristics can be used.

[0043] The valve 101, the sensor 100 and/or the RF tag 114 and masking element 115 can also optionally include a coating 116 that is adapted to hermetically seal all or at least a portion of the RF tag 114 and/or masking element 115. The coating 116 can be applied to only a portion of the RF tag 114 and/or masking element 115 that could be exposed to fluid. The RF tag 114 and the sensor 100 can be coated separately, with different coatings, or together in a single coating. An adhesive or other mating technique can optionally be used to affix the RF tag 114 and/or masking element 115 within the reservoir 108, however, in some embodiments it can be useful to allow the RF tag 114 and/or masking element 115 to be removed from the sensor 100 if necessary. Alternatively, the sensor 100 can be coated after the RF tag 114 and/or masking element 115 are disposed in the reservoir 108 to form a protective sheath. The ports 106, 110 can be protected from any coating applied thereto, formed after the coating is applied, or be cleared of any coating applied thereto to allow fluid to flow therethrough. In other embodiments, only certain components of the sensor 100 can be coated. A person skilled in the art will appreciate that a variety of other techniques can be used to seal the components of the sensor 100.

[0044] The material used to form the coating 116 can vary, and a variety of techniques can be used to apply the coating. By way of non-limiting example, suitable materials include polyurethane, silicone, solvent-based polymer solutions, and any other polymer that will adhere to the components to which it is applied to, and suitable techniques for applying the coating include spray-coating or dip-coating.

[0045] FIG. 10 shows one exemplary embodiment of a reading device 1000, such as an RF telemetry device, for use in obtaining information from the RF tag 114. The reading device 1000 can emit a signal at one frequency or over a range of frequencies, and can listen for the response thereto, e.g., from the RF tag 114. In the case of a chipless RF tag, a characteristic of the response from the tag can indicate a measured flow rate, as explained previously. In the case of a chip-based RF tag having memory associated therewith, the response of the tag can communicate information (e.g., according to a communication protocol) stored in its memory for the reading device. Any type of external reading device can be used. In one exemplary embodiment, the reading device 1000 can include an RF module (e.g., transmitter and receiver), a control unit (e.g., microcontroller), a coupling element to the transponder (e.g., antenna), and an interface (e.g., Recommended Standard (RS) 232, RS-485, Firewire, Universal Serial Bus (USB), Bluetooth, ZigBee, etc.) to enable communication with another device (e.g., a personal computer). The reading device 1000 can provide the power required by the RF tag 114 to operate, e.g., via inductive coupling. As shown in FIG. 11, the reading device 1000 can be positioned in proximity to an implanted RF tag 114 to telemetrically communicate with the RF tag 114, and thereby obtain a reading of the measured flow rate.

[0046] In another aspect, a method for measuring a rate of fluid flow is provided. In one embodiment, an exemplary method can include implanting a flow sensor, such as the flow sensor 100 described above in connection with FIGS. 1A and 1B, in a body. In the case of a hydrocephalus shunt, a hydrocephalus valve including the flow sensor can be subcutaneously implanted in a patient, as shown in FIG. 11. It should be understood that while FIG. 12 shows the implantation of a flow sensor in a shoulder region, the device can be implanted virtually anywhere, for example subcutaneously behind the ear, or on the head, torso, etc. The method can also include coupling a proximal end of a catheter, such as a ventricular catheter, to an inlet port of the flow sensor. Another catheter, such as a drainage catheter, can be coupled to an outlet port of the flow sensor. The drainage catheter can extend through the patient to an area where excess fluid, e.g., CSF, can drain safely.

[0047] The method can further include wirelessly transmitting a wireless signal to an RF tag embedded in the flow sensor, for example using a reading device such as reading device 1000 described above in connection with FIG. 10. The transmitted signal can include one or more

frequencies. In some embodiments, the wireless signal can be transmitted according to a protocol in order to communicate with an RF tag having a chip therein. The method can also include receiving a response from the RF tag that indicates a rate of fluid flowing through the sensor housing. The response can have one or more characteristics, such as resonance frequency, harmonic spectra, decay characteristics, and Q factor, that can be detected and analyzed in order to determine a measured rate of flow. In some embodiments, the response from the RF tag can be static, not changing over time unless the rate of fluid flow changes. In other embodiments, the response from the RF tag can exhibit periodicity, and analysis of the response can include determining a rate of flow based on the periodicity of the response signal. The determination of a flow rate can be performed using calibration data for a particular flow sensor. In some embodiments, the calibration data, as well as other data such as identification and/or historical data, can be transmitted from an RF tag having a memory to the reading device.

[0048] Further information on wireless shunts can be obtained from U.S. Patent Application No. _____, entitled "Wireless Pressure Setting Indicator" by Salim Kassem (Attorney Docket No. 22719-90 (COD-5163USNP)), U.S. Patent Application No. _____, entitled "Wireless Pressure Sensing Shunts" by Salim Kassem (Attorney Docket No. 22719-92 (COD-5160USNP)), and U.S. Patent Application No. _____, entitled "Wireless Shunts With Storage" by Salim Kassem (Attorney Docket No. 22719-93 (COD-5176USNP)), all of which are being filed on the same date as the present application and which are hereby incorporated by reference in their entirety. Also incorporated by reference in its entirety is co-pending, commonly assigned U.S. Patent Application No. 10/907,665, entitled "Pressure Sensing Valve" and published as U.S. Publication No. 2006-0211946 A1.

[0049] A person skilled in the art will appreciate that the various methods and devices disclosed herein can be formed from a variety of materials. Moreover, particular components can be implantable and in such embodiments the components can be formed from various biocompatible materials known in the art. Exemplary biocompatible materials include, by way of non-limiting example, composite plastic materials, biocompatible metals and alloys such as stainless steel, titanium, titanium alloys and cobalt-chromium alloys, glass, and any other material that is biologically compatible and non-toxic to the human body.

[0050] One skilled in the art will appreciate further features and advantages based on the above-described embodiments. Accordingly, the disclosure is not to be limited by what has been particularly shown and described, except as indicated by the appended claims. All publications and references cited herein are expressly incorporated herein by reference in their entirety.

[0051] What is claimed is:

REIVINDICACIONES

1. Un sensor implantable para medir flujo de líquidos, que comprende:

Una carcasa de sensor adaptada para recibir un flujo de líquido;

Un marcador de radiofrecuencia colocado dentro de la carcasa de sensor y adaptado para interactuar con una señal inalámbrica y producir una respuesta; y

Un elemento de máscara dispuesto en la carcasa del sensor, el elemento de máscara y el marcador de radiofrecuencia se configuran para moverse con relación uno al otro para alterar la respuesta del marcador de radiofrecuencia e indicar por lo tanto una tasa de líquido que fluye a través de la carcasa de sensor

2. El sensor implantable de la reivindicación 1, en donde el elemento de máscara comprende un miembro conductor que altera la respuesta del marcador de radiofrecuencia.

3. El sensor implantable de la reivindicación 2, en donde el elemento de máscara cubre por lo menos una porción del marcador de radiofrecuencia.
4. El sensor implantable de la reivindicación 1, en donde por lo menos una característica de la respuesta corresponde a la tasa de flujo, por lo menos una característica que se selecciona del grupo que consiste de: una frecuencia de resonancia, espectro armónico, característica de desgaste, y factor Q.
5. El sensor implantable de la reivindicación 1, que comprende adicionalmente un montaje de válvula adaptado para controlar una tasa de líquido que fluye a través de la carcasa del sensor, el montaje de válvula está en comunicación fluida con la carcasa del sensor.
6. El sensor implantable de la reivindicación 1, en donde el elemento de máscara se configura para rotar alrededor de un eje de éste en relación con la tasa de flujo del líquido a través de la carcasa del sensor.
7. El sensor implantable e la reivindicación 6, en donde el elemento de máscara comprende un disco formado por lo

menos en parte de un material conductor para enmascarar selectivamente parte del marcador de radiofrecuencia, el elemento de máscara se configura para rotar alrededor de un eje de este para enmascarar diferentes partes del marcador de radiofrecuencia de tal manera que la respuesta del marcador de radiofrecuencia para la señal inalámbrica sea periódica.

8. El sensor implantable e la reivindicación 7, en donde la parte del disco formado del material conductor tienen una forma que se selecciona del grupo que consiste de un espiral y una pluralidad de secciones conductoras discretas.
9. El sensor implantable de la reivindicación 1, en donde el marcador de radiofrecuencia comprende un disco que tiene una antena asimétrica, el elemento de máscara se configura para enmascarar por lo menos parte de la antena.
10. El sensor implantable de la reivindicación 1, donde el elemento de máscara comprende una cuña formada por lo menos en parte de un material conductor y el elemento de máscara se configura para trasladarse en relación con la

tasa de flujo de líquido a través de la carcasa del sensor

11. un sensor implantable, que comprende:

Una carcasa de sensor adaptada para recibir flujo de líquido;

Un miembro conductor dispuesto dentro del montaje de válvula y configurado para cubrir selectivamente por lo menos una porción de un marcador de radiofrecuencia y por lo tanto alterar una respuesta de éste a una señal inalámbrica recibida para indicar una tasa de líquido que fluye a través de la carcasa del sensor.

- 12 Un sensor implantable de la reivindicación 11, en donde la respuesta tiene por los menos una característica que se puede medir seleccionada del grupo que consiste de frecuencia de resonancia, espectro armónico, características de desgaste, y factor Q.
- 13 Un sensor implantable de la reivindicación 11, en donde el miembro conductor se configura para moverse con relación al marcador de radiofrecuencia,

- 14 Un sensor implantable de la reivindicación 11, en donde el marcador de radiofrecuencia se configura para moverse con relación al miembro conductor.
- 15 Un sensor implantable de la reivindicación 14, en donde el marcador de radiofrecuencia comprende un disco que tienen una antena asimétrica formada allí.
- 16 Un sensor implantable de la reivindicación 11, que comprende adicionalmente un montaje de válvula adaptado para controlar una tasa de líquido que fluye a través de la carcasa del sensor, el montaje de válvula está en comunicación fluida con la carcasa del sensor.
- 17 Un sensor implantable de la reivindicación 11, en donde los miembros conductores forman parte de un disco que puede rotar.
- 18 Un método para medir el flujo de líquido, comprende:
- posicionar una carcasa de sensor entre un tubo de entrada y un tubo de salida, la carcasa del sensor tiene un marcador de radiofrecuencia colocado allí;

Trasmitir una señal inalámbrica a un marcador de radiofrecuencia colocado dentro de una carcasa de sensor que tiene un líquido que fluye a través de este desde un dispositivo de lectura; y

Recibir en forma inalámbrica una respuesta desde el marcador de radiofrecuencia que indica la tasa del líquido que fluye a través de la carcasa de sensor.

19 El método de la reivindicación 18, en donde la respuesta recibida del marcador de radiofrecuencia cambia con relación a la tasa de líquido que fluye a través de la carcasa de sensor.

20 El método de la reivindicación 18, que comprende adicionalmente acoplar un tubo de entrada acoplado con la carcasa de sensor para un catéter dentro de un ventrículo de un paciente, y acoplar un tubo de salida acoplado con la carcasa de sensor para un catéter de drenaje para drenar el líquido cefalorraquídeo del paciente.

- 21 El método de la reivindicación 18, que comprende adicionalmente acoplar la carcasa de sensor con un montaje de válvula adaptado para controlar una tasa de líquido que fluye a través de la carcasa de sensor.
- 22 El método de la reivindicación 18, en donde la respuesta del marcador de la radiofrecuencia es una señal periódica
- 23 El método de la reivindicación 18, que comprende adicionalmente analizar la respuesta para detectar cualquiera de frecuencia de resonancia, espectro armónico, características de desgaste y factor Q del marcador de radiofrecuencia.
- 24 El método de la reivindicación 18, que comprende adicionalmente recibir una respuesta del marcador de radiofrecuencia que comunica los datos previamente almacenados allí.

CLAIMS:

1. An implantable sensor for measuring fluid flow, comprising:
a sensor housing adapted to receive fluid flow therethrough;
a radio frequency tag disposed within the sensor housing and adapted to interact with a wireless signal and to produce a response thereto; and
a masking element disposed in the sensor housing, the masking element and the radio frequency tag configured to move relative to one another to alter the response of the radio frequency tag and thereby indicate a rate of fluid flowing through the sensor housing.
2. The implantable sensor of claim 1, wherein the masking element comprises a conductive member that alters the response of the radio frequency tag.
3. The implantable sensor of claim 2, wherein the masking element covers at least a portion of the radio frequency tag.
4. The implantable sensor of claim 1, wherein at least one characteristic of the response corresponds to the flow rate, the at least one characteristic being selected from the group consisting of: resonant frequency, harmonic spectra, decay characteristic, and Q factor.
5. The implantable sensor of claim 1, further comprising a valve assembly adapted to control a rate of fluid flowing through the sensor housing, the valve assembly being in fluid communication with the sensor housing.
6. The implantable sensor of claim 1, wherein the masking element is configured to rotate around an axis thereof in relation to the flow rate of fluid through the sensor housing.
7. The implantable sensor of claim 6, wherein the masking element comprises a disk formed at least in part of a conductive material to selectively mask part of the radio frequency tag, the masking element being configured to rotate around an axis thereof to mask different parts of the radio frequency tag such that the response of the radio frequency tag to the wireless signal is periodic.

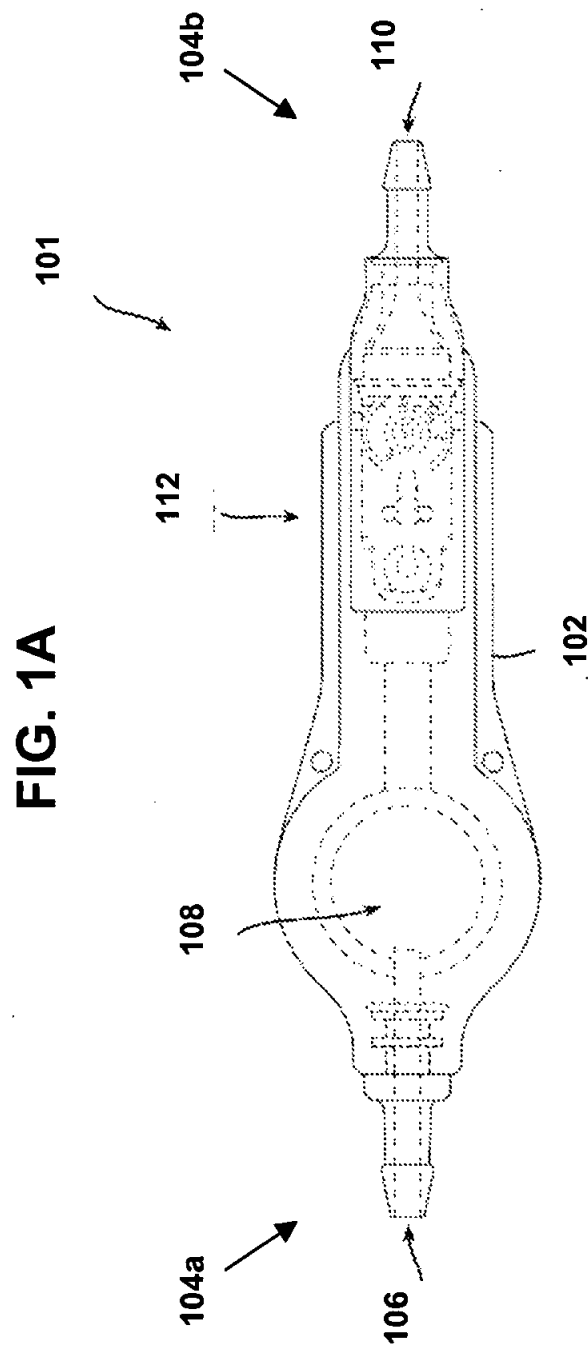
8. The implantable sensor of claim 7, wherein the part of the disk formed of the conductive material has a shape that is selected from the group consisting of a spiral and a plurality of discrete conductive sections.
9. The implantable sensor of claim 1, wherein the radio frequency tag comprises a disk having an asymmetrical antenna, the masking element configured to mask at least part of the antenna.
10. The implantable sensor of claim 1, wherein the masking element comprises a wedge formed at least in part of a conductive material and the masking element is configured to translate in relation to the flow rate of fluid through the sensor housing.
11. An implantable sensor, comprising:
 - a sensor housing adapted to receive fluid flow therethrough; and
 - a conductive member disposed within the valve assembly and configured to selectively cover at least a portion of a radio frequency tag and thereby alter a response thereof to a received wireless signal to indicate a rate of fluid flowing through the sensor housing.
12. The implantable sensor of claim 11, wherein the response has at least one measurable characteristic selected from the group consisting of resonant frequency, harmonic spectra, decay characteristic, and Q factor.
13. The implantable sensor of claim 11, wherein the conductive member is configured to move relative to the radio frequency tag.
14. The implantable sensor of claim 11, wherein the radio frequency tag is configured to move relative to the conductive member.
15. The implantable sensor of claim 14, wherein the radio frequency tag comprises a disk having an asymmetrical antenna formed thereon.
16. The implantable sensor of claim 11, further comprising a valve assembly adapted to control a rate of fluid flowing through the sensor housing, the valve assembly being in fluid communication with the sensor housing.

17. The implantable sensor of claim 11, wherein the conductive member forms part of a rotatable disk.
18. A method for measuring fluid flow, comprising:
positioning a sensor housing between an inlet tube and an outlet tube, the sensor housing having a radio frequency tag disposed therein;
transmitting a wireless signal to a radio frequency tag disposed within a sensor housing having fluid flowing therethrough from a reading device; and
wirelessly receiving a response from the radio frequency tag that indicates a rate of fluid flowing through the sensor housing.
19. The method of claim 18, wherein the response received from the radio frequency tag changes in relation to the rate of fluid flowing through the sensor housing.
20. The method of claim 18, further comprising coupling an inlet tube mated to the sensor housing to a catheter within a patient's ventricle, and coupling an outlet tube mated to the sensor housing to a drainage catheter for draining the patient's cerebrospinal fluid.
21. The method of claim 18, further comprising coupling the sensor housing to a valve assembly adapted to control a rate of fluid flowing through the sensor housing.
22. The method of claim 18, wherein the response from the radio frequency tag is a periodic signal.
23. The method of claim 18, further comprising analyzing the response to detect any of resonant frequency, harmonic spectra, decay characteristic, and Q factor of the radio frequency tag.
24. The method of claim 18, further comprising receiving a response from the radio frequency tag that communicates data previously stored therein.

ABSTRACT

Devices and methods useful for non-invasively measuring and indicating a rate of fluid flow are disclosed. In one embodiment, a sensor housing adapted to received fluid flow therethrough is provided. A radio frequency tag and a masking element can be disposed in the sensor housing. The masking element and the radio frequency tag can be configured to move relative to one another. The relative positions or movement can alter the response of the radio frequency tag to a wireless signal (which can be emitted from an external reading device, for example) and thereby indicate a rate of fluid flowing through the housing. For example, in some embodiments, the masking element can selectively cover at least part of the radio frequency tag in correspondence to the flow rate, which can change a characteristic of the radio frequency tag's response to the wireless signal.

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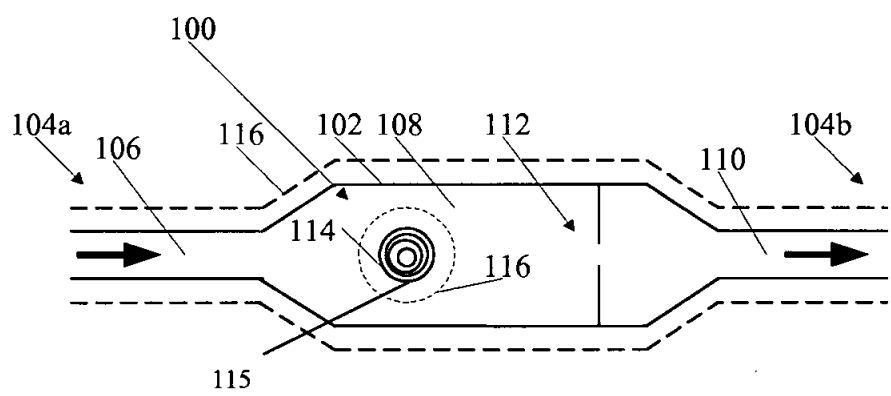


FIG. 2A

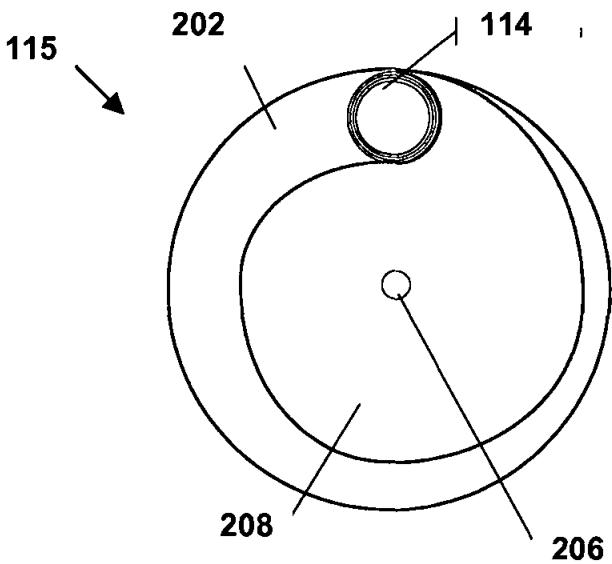


FIG. 2B

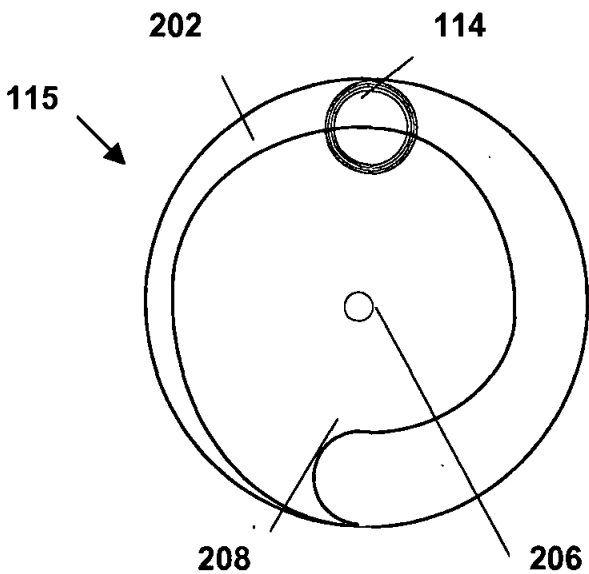


FIG. 3

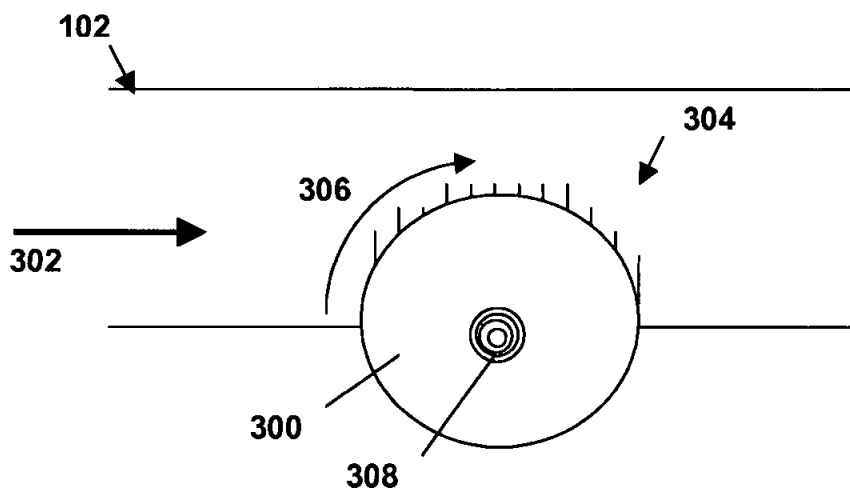


FIG. 4

400

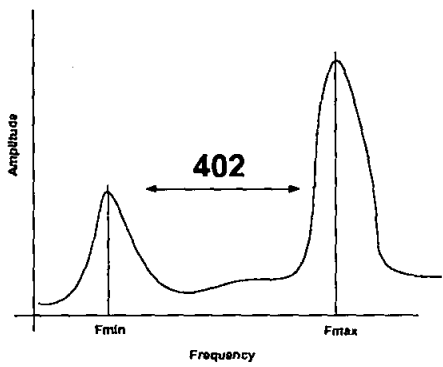


FIG. 5

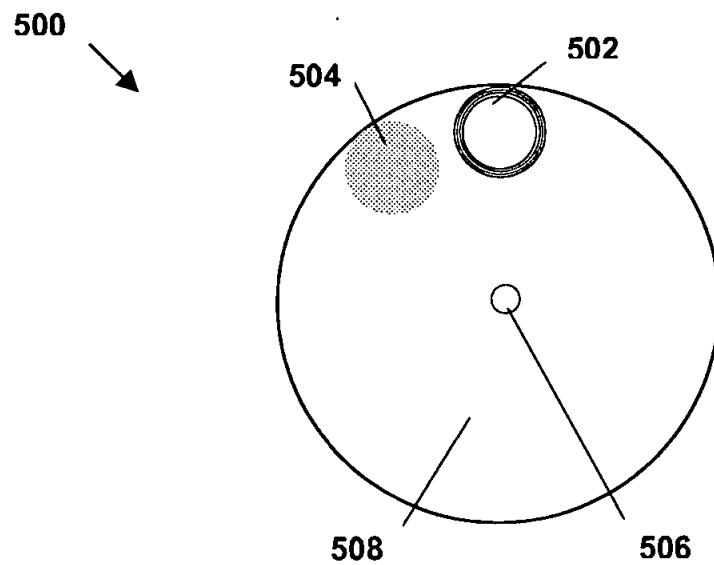


FIG. 6

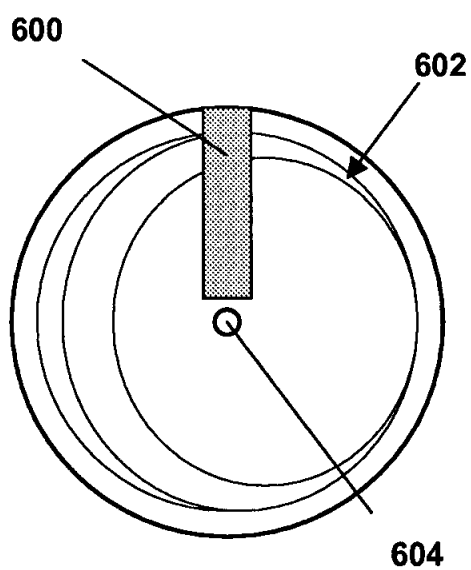


FIG. 7A

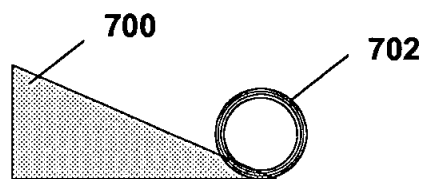


FIG. 7B

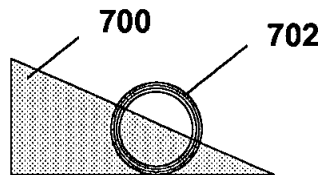
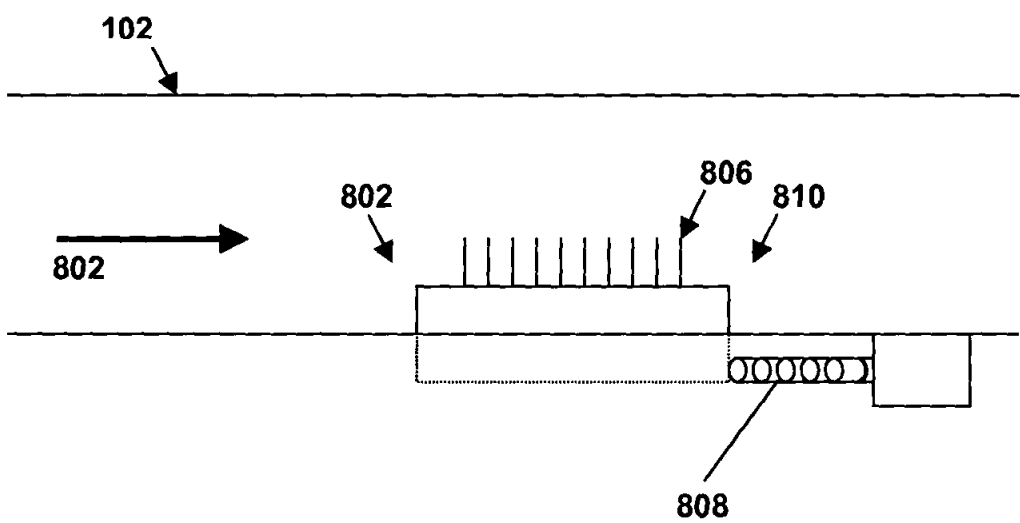


FIG. 8



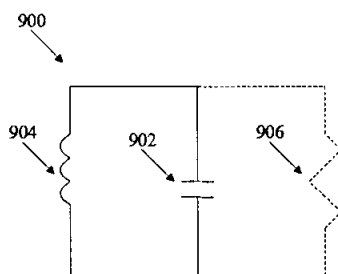


FIG. 9A

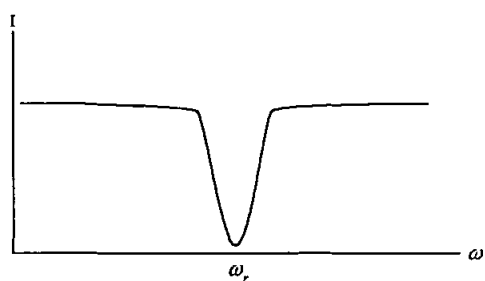


FIG. 9B

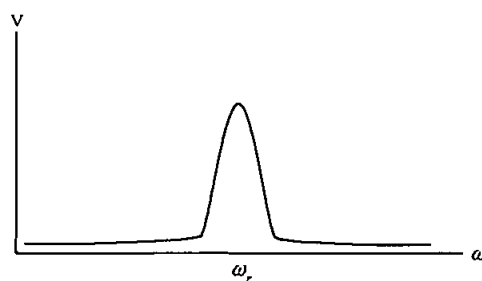
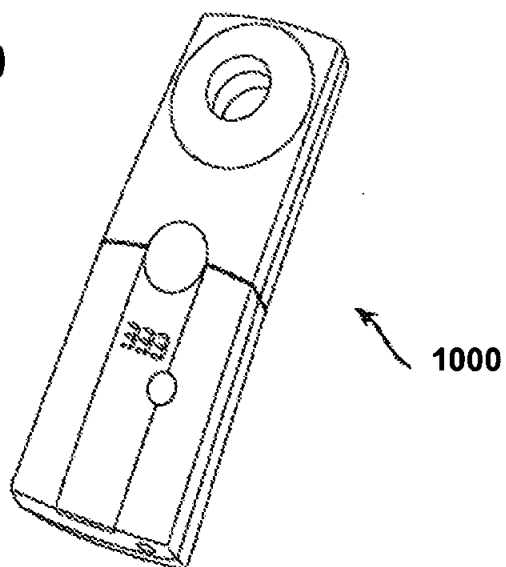


FIG. 9C

FIG. 10



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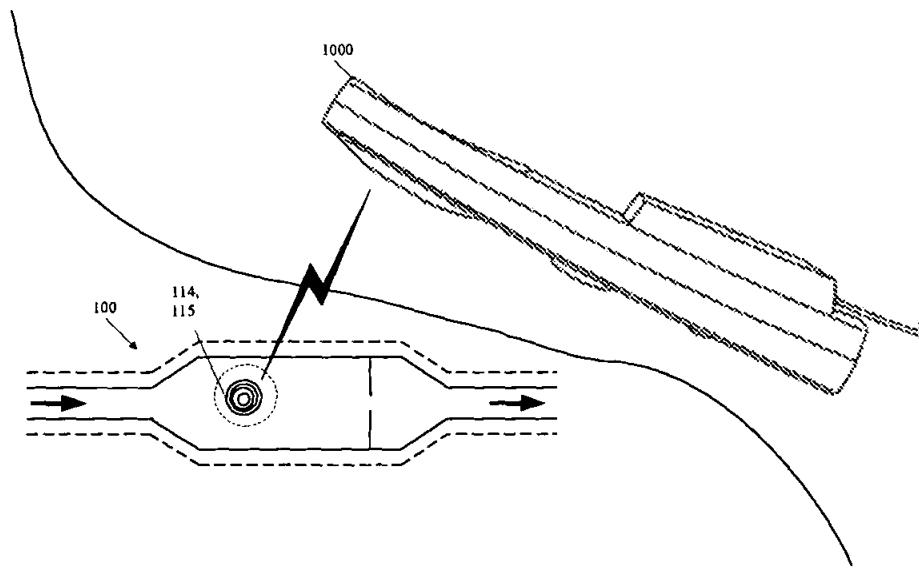


FIG. 11